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Abbreviated Abstract

We aim with this original article to develop, validate, and compare three deep transfer learning algorithms to predict between in situ or invasive melanoma and < 0.8 or \hat{a} % ¥ 0.8 millimetres of Breslow thickness.

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Title page

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21 22	Bullet statements:
23 24 25	'What is already known about this topic?'
26 27	• Previous studies assessed the prediction of CNN for the comparison between in
28 29	situ or invasive melanoma using ResNet50 and <i>de novo</i> CNN.
30 31 32	'What does this study add?'
33 34	• This study compared three DTL pretrained CNN and dermatologist performance
35 36	predicting in situ versus invasive melanoma and $<$ or ≥ 0.8 millimetres of Breslow
37 38	thickness.
40 41	• DTL could be an ancillary aid to support dermatologists' decision in the near
42 43	future.
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Abstract

Background: The distinction between in situ (MIS) or invasive melanoma is challenging even for expert dermatologists. The use of pretrained convolutional neural networks (CNNs) as ancillary decision systems needs further research.

Objective: To develop, validate and compare three deep transfer learning algorithms to predict between MIS or invasive melanoma and $< \text{ or } \ge 0.8$ millimetres of Breslow thickness (BT).

Methods: A dataset of 1,315 dermoscopic images of histopathologically confirmed melanomas was created from Virgen del Rocio University Hospital and open repositories of the ISIC archive and Polesie et al. The images were labelled as MIS or invasive melanoma and < or ≥ 0.8 millimetres of BT. We conducted three trainings, and overall means for ROC curves, sensitivity, specificity, positive and negative predictive value, and balanced diagnostic accuracy outcomes were evaluated on the test set with ResNetV2, EfficientNetB6, and InceptionV3. The results of ten dermatologists were compared with the algorithms. Grad-CAM gradient maps were generated, highlighting relevant areas considered by the CNNs within the images.

Results: EfficientNetB6 achieved the highest diagnostic accuracy for the comparison between MIS and invasive melanoma, and < 0.8 versus ≥ 0.8 of BT were 61% and 75%, respectively. For the latter, ResNetV2, with an area under the ROC curve of 0.76, and EfficientNetB6, of 0.79, outperformed the results obtained by the dermatologist group with 0.70.

Conclusions: EfficientNetB6 recorded the best prediction results, overcoming dermatologists for the comparison of 0.8 mm of BT. DTL could be an ancillary aid to support dermatologists' decision in the near future.

Introduction

Cutaneous melanoma is responsible for almost 90% of skin cancer deaths, worsening the prognosis when diagnosis is delayed¹. Breslow thickness (BT) is the main prognostic factor in primary cutaneous melanoma, which measures the microinvasion of the tumour in millimetres (mm) from the granular layer to the deepest of tumour invasion². In addition to ulceration, BT sets out the T classification of 8thAJCC¹.

An accurate diagnosis of early melanoma is one of the major goals of dermoscopy³, but distinction between in situ (MIS) and invasive melanoma could be challenging even for expert dermatologist⁴.

Deep learning methods are a novel approach for the diagnosis of melanoma, which uses convolutional neural networks (CNNs) to computationally analyse dermoscopic images⁵. One of the drawbacks of deep learning is the need for large amounts of training data to complex patterns within images. To address this issue, deep transfer learning (DTL) is a technique that allows training of CNNs with a lower amount of data, using previous learned model knowledge with minimum training or fine-tuning to perform a new task⁶. To discriminate between MIS and invasive melanoma, some authors created *de novo* CNNs^{7–10}, but only one pretrained ResNet50 CNN model was previously used for this comparison^{10,11}. Human readers outperformed *de novo* CNNs, but not the pretrained CNN¹⁰, so the scope of pretrained CNNs to differentiate MIS versus invasive melanoma

should be further analysed.

To our knowledge, no studies compared different DTL approaches using pretrained CNNs. This study aimed to develop, validate, and compare three DTL algorithms to predict whether a melanoma is MIS or invasive and whether the BT is < 0.8 or ≥ 0.8 mm,

based on dermoscopic images. Also, we aimed to compare the performance of human readers with that of DTL algorithms.

Material and methods

This retrospective study was performed according to the Declaration of Helsinki and the Standards for Reporting Diagnostic Accuracy (STARD). The Andalusian Review Board and Ethics Committee Virgen Macarena-Virgen del Rocio Hospitals approved the study protocol (ID 0096-N-20). The main dataset was composed of dermoscopic images of histopathologically confirmed melanomas in which BT was measured. To increase clinical relevance, we did not restrict the melanoma subtype or subjects' phototype¹².

Three independent subsets made up our dataset: (i) 1,055 images of 279 cases from the dermoscopic image repository of Virgen del Rocio University Hospital (Seville, Spain) between 2016 and 2022 (Supplemental material); (ii) 193 images of 184 cases from Polesie et al.¹³ (iii) 67 images of 67 cases from the ISIC archive¹⁴. In the (i) and (ii) subsets, some cases had more than one image. These were discarded from the validation and test datasets, but not from the training dataset since it improves training performance. Upsampling was conducted to prevent a higher weight being conferred on cases with more than one image. Thus, we built synthetic copies up to equalling 10 images per case.

Image labelling

The ground truth was established by histopathological diagnosis. Each image was labelled as MIS or invasive melanoma, and < 0.8 or ≥ 0.8 mm of BT. We considered 0.8 mm of BT, as it is the threshold in Europe to perform a sentinel lymph node biopsy, when associating with additional histological risk factors as ulceration¹⁵. To assess CNNs prediction potential, we performed two comparisons, MIS (283 images) versus invasive melanoma (1,032 images) and < 0.8 (702 images) versus ≥ 0.8 mm (613 images) of BT.

Image subsets and overfitting prevention

The 80% of the images were used for the training dataset, 10% for validation, and 10% for the test dataset. A cross-validation was not possible since some of our cases comprised more than one image. Instead, we performed the Dropout Regularization¹⁶ and an external test dataset. Also, we conducted 3 trainings with the same test dataset, and the overall means for all outcomes were calculated.

CNN architecture

To train the different CNNs, we resized all images to an appropriate input size, using 299 x 299 pixels for ResNetV2 and InceptionV3, and 512 x 512 pixels for EfficientNetB6. To enhance the external validity to real clinical settings, we did not use any software to modify or curate the dermoscopic images.

As we used different numbers of images per class within each training dataset, the distribution of labelled images in each subset was imbalanced. To solve this, we performed the weight assignment with the *class_weight* function from Keras¹⁷. To optimize training performance, we established parameters like exponential learning rate scheduler, and callbacks to save model parameters and to perform an early stopping (*monitor='val_loss', patience=10*). To avoid overfitting, we used data augmentation with the following transformations: *rotation_range=40, width_shift_range=0.2, horizontal flip=True.*

Gradient maps

To make CNNs output comprehensible, we created gradient maps with the Gradientweighted Class Activation Mapping (Grad-CAM)¹⁸. Grad-CAM is a technique of computer vision that remarks the region of interest of the input images that are relevant for the prediction of a CNN model.

Statistical analysis

The R software (v.4.1.2) was used to perform all statistical analyses. The capacity to differentiate classes (MIS or invasive, and < or ≥ 0.8 mm of BT) inferred by the model was used to calculate the receiver operating characteristic (ROC) curves. To calculate the ROC curves with 95% confidence intervals, we used the package "nsROC" (v.1.1)¹⁹. Sensitivity, specificity, positive and negative predictive value, and balanced diagnostic accuracy outcomes were evaluated for each CNN. To examine the performance of the model, we compared the prediction outcomes obtained with those achieved by 5 board-certified dermatologists and 5 dermatology residents. All human readers independently performed predictions for the same test datasets evaluated by all the CNN models. To calculate the interobserver agreement we used the Fleiss' kappa index (k)²⁰.

Results

We compared 3 pretrained CNNs, which test set performance is shown in Table 1. The test set for the comparison between MIS and invasive melanoma (n = 111 images) consisted of 51 MIS and 59 invasive melanomas. The test set for the comparison between melanoma $< \text{ or } \ge 0.8 \text{ BT}$ (n = 86) was constituted by 55 and 31 cases, respectively.

For the MIS versus invasive melanoma prediction model, EfficientNetB6 presented the highest diagnostic accuracy (61%) and sensitivity (72%), whilst it performed the lowest specificity value (31%) of the three pretrained models. The mean area under the ROC curve (AUC) was 0.59, 0.63 and 0.54 for ResNetV2, InceptionV3 and EfficientNetB6, respectively (Figure 1). The readers outperformed the three models for this comparison, showing a diagnostic accuracy of 64% and an AUC of 0.64 (Table 2). Interobserver agreement of dermatologists for this comparison was moderate, k = 0.46.

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In the assessment of invasive melanomas ≥ 0.8 mm of BT, EfficientNetB6 achieved the highest diagnostic accuracy (84%) and specificity (84%). This CNN model recorded a sensitivity of 58%, being the lowest value compared to the 60% and 65% achieved by ResNetV2 and InceptionV3, respectively. The mean AUC was 0.76, 0.75 and 0.69 for ResNetV2, InceptionV3, and EfficientNetB6, respectively (Figure 2). For this comparison, the mean diagnostic accuracy achieved by the dermatologist was 69%, with an AUC of 0.70 (Table 2). Interobserver agreement of dermatologists was fair, k = 0.35. Radar charts illustrated the juxtaposition of the main results to compare the performance of each pretrained CNN model and dermatologists (Figure 3).

Gradient maps

Gradient maps spotlight influential areas of dermoscopic images, where the red colour remarks high attribution area for a specific prediction (Figure 4). Figure 4 remarks gradient map examples of a true positive (TP), true negative (TN), false positive (FP), and false negative (FN) dermoscopic image.

Discussion

This study analysed the performance of three DTL models for the prediction of microinvasion using melanoma dermoscopic images. EfficientNetB6 achieved the highest diagnostic accuracy for the comparison between MIS and invasive melanoma, and < 0.8 versus ≥ 0.8 of BT. For the latter, ResNetV2 and EfficientNetB6 outperformed the dermatologist group.

The state of the art related to the use of deep learning as a decision support system has grown in recent years. Most of the studies that focused on the differentiation between MIS and invasive, developed, and implemented a *de novo* CNN; only Polesie et al.¹⁰ and Chu et al.¹¹ used a pretrained ResNet50 CNN. The first author tested CNN performance

on a dataset of 523 dermoscopic images, achieving an AUC of 0.83. This result was not significantly outperformed by 438 international readers for the comparison between MIS and invasive, who reached an AUC of 0.85. The AUC results in this study were superior to ours in the three pretrained CNNs, but it should be noted that our dermatologists did not receive any baseline educational program prior to discrimination of dermoscopic images. This was conducted to avoid recall bias and to match the research context with daily clinical practice.

Chu et al.¹¹ used ResNet50 to differentiate between MIS and invasive and depth of microinvasion, but in acral lentiginous melanoma. Despite being in a different clinical setting, the CNN performed effectively to distinguish between < 0.8 mm and ≥ 0.8 mm of BT, with and AUC of 0.90 in 57 dermoscopic images. Similarly, we achieved favourable results to discriminate between MIS and invasive and for the level of microinvasion.

Regarding *de novo* CNNs, all studies recorded a fair to moderate accuracy for the distinction between MIS and invasive melanoma like the performance of our pretrained CNNs. *De* novo CNNs were not superior to dermatologists in the classification of MIS or invasive melanoma, whereas only pretrained CNNs outperformed them, as Polesie et al.¹⁰ confirmed. This could help to achieve early detection and accurate stratification at the time of diagnosis. In our results, pretrained CNNs performed better for the prediction of melanomas ≥ 0.8 mm of BT, possibly related to the fact that most of the dermoscopic features between MIS and thin melanomas are overlapped²¹.

In addition to similar performance as *de novo* CNNs and outperformance versus dermatologists to predict between MIS and invasive melanoma, further advantages of pretrained CNNs compared to *de novo* have been reported in the scientific literature. DTL uses open code pretrained CNNs that store the information images from other problems

and utilize for a different target. Additionally, it presents better image feature extraction, lower sample size and shorter time for the learning process, making DTL an optimal tool to obtain quicker and more cost-effective results in healthcare²².

Clinical and research implications

Our pretrained CNNs appears to be useful ancillary aids in selecting the optimal surgical approach and tumour staging in cutaneous melanoma based on the threshold of 0.8 mm BT. The implementation of CNNs in the dermatology field could help to support the triage and prioritize early cases. A recent study confirmed that most patients were open to CNN use in diagnosis, but always under dermatology supervision²³. Within the research framework, the implementation of these CNN needs to be prospectively examined in the real-world clinical setting. Also, a call for action is needed for the standardisation of dermoscopic imaging that could lead to robust results of algorithms. We propose attaching the DICOM standard (supplement 221)²⁴, which suggests adding metadata to images, so the CNN could handle patient data to make the prediction as dermatologists NC. make in their daily practice.

Limitations

A major pitfall of our dermoscopic image repository, found in the background literature, is that people with skin of colour were not involved. Thus, as Butt et al.²⁵ declared it is imperative to conduct future studies in this population, to avoid racial bias and to evaluate CNN performance. Due to the retrospective design of the study, patient metadata was not available to be included in the dermoscopic image.

Conclusions

This study showed a suitable prediction of three pretrained CNN for discrimination between MIS and invasive melanoma and for the distinction between a BT < 0.8 and \geq

0.8 mm, using 1,315 dermoscopic images. For both models, EfficientNetB6 recorded the best prediction results, overcoming dermatologists for the comparison of 0.8 mm of BT. DTL could be an ancillary aid to support dermatologists' decision in the near future. Nevertheless, a standardisation on dermoscopic images is necessary to achieve the best output of CNN.

Acknowledgments

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Data availability

The data underlying this article will be shared on reasonable request to the corresponding author.

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Supporting information:

The CNNs code can be found at

<u>https://github.com/juaherrod/UHVR_DERMOSCOPY_BRESLOW</u>. The dataset of dermoscopic images from Virgen del Rocio University Hospital is available as online supplementary material.

Figure legends:

Figure 1. ROC curves for the prediction model between in situ and invasive melanoma for (a) ResNetV2, (b) InceptionV3 and (c) EfficientNetB6.

Figure 2. ROC curves for the prediction model between melanoma < 0.8 or ≥ 0.8 mm of Breslow thickness for (a) ResNetV2, (b) InceptionV3 and (c) EfficientNetB6.

Figure 3. Radar Chart for the comparison of the performance of the three pretrained CNN for (a) MIS vs invasive melanoma and (b) melanoma $< 0.8 \text{ mm or } \ge 0.8 \text{ mm of BT}$.

Figure 4. Gradient maps. (a) True positive (TP): the algorithm identified a blue-white veil area as an important region of a melanoma ≥ 0.8 BT. (b) True negative (TN): a regular network area was identified by the algorithm to predict a melanoma < 0.8 mm BT. (c) False positive (FP): the algorithm focused on the healthy surrounding skin of a tiny nodular melanoma ≥ 0.8 mm. (d) False negative (FN): the algorithm was unable to focus on a specific dermoscopic structure to correctly perform the prediction in a melanoma < 0.8 mm BT.

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Comparison	Training	Se	Sp	PPV	NPV	Accuracy	F1-	AUC
_	dataset		_			_	score	
	ResNetV2	0.61 ± 0.15	0.50 ± 0.14	0.66 ± 0.15	0.45 ± 0.19	0.54 ± 0.02	0.61 ± 0.01	0.59 ± 0.03
In situ vs Invasive	InceptionV3	0.63 ± 0.13	0.51 ± 0.12	0.68 ± 0.14	0.45 ± 0.14	$\begin{array}{c} 0.56 \pm \\ 0.03 \end{array}$	0.64 ± 0,04	0.63 ± 0.02
	EfficientNetB6	$\begin{array}{c} 0.72 \pm \\ 0.03 \end{array}$	0.39 ± 0.04	0.70 ± 0.04	0.41 ± 0.09	0.61 ± 0.02	0.71 ± 0.01	0.54 ± 0.06
	ResNetV2	0.60 ± 0.17	0.76 ± 0.08	0.57 ± 0.07	0.79 ± 0.11	$\begin{array}{c} 0.70 \pm \\ 0.04 \end{array}$	0.57 ± 0.04	0.76 ± 0.06
	InceptionV3	0.65 ± 0.22	0.70 ± 0.14	0.53 ± 0.17	0.79 ± 0.17	$\begin{array}{c} 0.65 \pm \\ 0.04 \end{array}$	0.54 ± 0.04	0.75 ± 0.01
	EfficientNetB6	0.58 ± 0.20	0.84 ± 0.06	0.61 ± 0.09	0.81 ± 0.10	0.75 ± 0.03	0.58 ± 0.09	0.69 ± 0.06

Table 1. Comparison of the Performance of Convolutional Neural Networks for prediction of melanoma Breslow thickness

AUC, area under the ROC curve; NPV, negative predictive value; PPV, positive predictive value; Se, sensitivity; Sp, specificity

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Readers	AUC	95%CI	Accuracy	Se
1	0.69	0.60 to 0.77	0.69	0.73
2	0.68	0.59 to 0.77	0.67	0.74
3	0.63	0.54 to 0.72	0.64	0.65
4	0.68	0.59 to 0.77	0.68	0.70
5	0.60	0.53 to 0.68	0.63	0.60
6	0.69	0.60 to 0.78	0.65	0.69
7	0.58	0.49 to 0.70	0.59	0.59
8	0.58	0.50 to 0.66	0.60	0.59
9	0.64	0.56 to 0.73	0.65	0.64
10	0.62	0.54 to 0.71	0.64	0.62
Mean	0.64	0.61 to 0.67	0.64	0.66
Melanoma < 0.8	$vs \ge 0.8$ millime	etres Breslow thickne	ess	
Readers	AUC	95%CI	Accuracy	Se
1	0.84	0.76 to 0.93	0.87	0.88
2	0.70	0.59 to 0.80	0.72	0.61
3	0.71	0.64 to 0.82	0.68	0.54
4	0.48	0.37 to 0.59	0.52	0.33
5	0.72	0.65 to 0.82	0.70	0.55
6	0.75	0.66 to 0.86	0.77	0.66
7	0.75	0.68 to 0.86	0.77	0.65
8	0.69	0.62 to 0.76	0.60	0.47
9	0.67	0.58 to 0.77	0.63	0.49
10	0.69	0.60 to 0.80	0.67	0.53
mean	0.70	0.64 to 0.76	0.69	0.57

Review





False-Positive Rate

ROC curves for the prediction model between in situ and invasive melanoma for (a) ResNetV2, (b) InceptionV3 and (c) EfficientNetB6.

232x167mm (144 x 144 DPI)





False-Positive Rate

ROC curves for the prediction model between in situ and invasive melanoma for (a) ResNetV2, (b) InceptionV3 and (c) EfficientNetB6.

236x169mm (144 x 144 DPI)





False-Positive Rate

ROC curves for the prediction model between in situ and invasive melanoma for (a) ResNetV2, (b) InceptionV3 and (c) EfficientNetB6.

236x166mm (144 x 144 DPI)

(a) ResNetV2



ROC curves for the prediction model between melanoma < 0.8 or \geq 0.8 mm of Breslow thickness for (a) ResNetV2, (b) InceptionV3 and (c) EfficientNetB6.

233x171mm (144 x 144 DPI)





False-Positive Rate

ROC curves for the prediction model between melanoma < 0.8 or \ge 0.8 mm of Breslow thickness for (a) ResNetV2, (b) InceptionV3 and (c) EfficientNetB6.

233x170mm (144 x 144 DPI)





False-Positive Rate

ROC curves for the prediction model between melanoma < 0.8 or \geq 0.8 mm of Breslow thickness for (a) ResNetV2, (b) InceptionV3 and (c) EfficientNetB6.

234x170mm (144 x 144 DPI)







Gradient maps. (a) True positive (TP): the algorithm identified a blue-white veil area as an important region of a melanoma ≥ 0.8 BT. (b) True negative (TN): a regular network area was identified by the algorithm to predict a melanoma < 0.8 mm BT. (c) False positive (FP): the algorithm focused on the healthy surrounding skin of a tiny nodular melanoma ≥ 0.8 mm. (d) False negative (FN): the algorithm was unable to focus on a specific dermoscopic structure to correctly perform the prediction in a melanoma < 0.8 mm BT.

338x190mm (96 x 96 DPI)



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